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ATTORNEY'S DOCKET NUMBER

TRANSMITTAL LETTER TO THE UNITED STATES
DESIGNATED/ELECTED OFFICE (DO/EO/US)
CONCERNING A FILING UNDER 35 U.S.C. 371

LEA 33 253

U.S. APPLICATION NO. (If known, see 37 CFR 1.5)

097787229

INTERNATIONAL APPLICATION NO.

PCT/EP99/06882

INTERNATIONAL FILING DATE

17 September 1999 (17.09.99)

PRIORITY DATE CLAIMED

18 September 1998 (18.09.98)

TITLE OF INVENTION MULTIPLE UNIT CONTROLLED FOOD EFFECT-INDEPENDENT RELEASE
PHARMACEUTICAL PREPARATIONS AND METHOD FOR PREPARING THE SAMEAPPLICANT(S) FOR DO/EO/US KANIKANTI, Venkata-Rangaro; RUPP, Roland; BRENDDEL, Erich;
WEISEMANN, Claus; CHANTRAINE, Ernst

Applicant herewith submits to the United States Designated/Elected Office (DO/EO/US) the following items and other information:

1. ☒ This is a **FIRST** submission of items concerning a filing under 35 U.S.C. 371.
2. ☐ This is a **SECOND** or **SUBSEQUENT** submission of items concerning a filing under 35 U.S.C. 371.
3. ☒ This express request to begin national examination procedures (35 U.S.C. 371(f)) at any time rather than delay examination until the expiration of the applicable time limit set in 35 U.S.C. 371(b) and PCT Articles 22 and 39(1).
4. ☒ A proper Demand for International Preliminary Examination was made by the 19th month from the earliest claimed priority date.
5. ☒ A copy of the International Application as filed (35 U.S.C. 371(c)(2))
 - a. ☒ is transmitted herewith (required only if not transmitted by the International Bureau).
 - b. ☐ has been transmitted by the International Bureau.
 - c. ☐ is not required, as the application was filed in the United States Receiving Office (RO/US).
6. ☒ A translation of the International Application into English (35 U.S.C. 371(c)(2)).
7. ☒ Amendments to the claims of the International Application under PCT Article 19 (35 U.S.C. 371(c)(3))
 - a. ☐ are transmitted herewith (required only if not transmitted by the International Bureau).
 - b. ☐ have been transmitted by the International Bureau.
 - c. ☐ have not been made; however, the time limit for making such amendments has NOT expired.
 - d. ☒ have not been made and will not be made.
8. ☐ A translation of the amendments to the claims under PCT Article 19 (35 U.S.C. 371(c)(3)).
9. ☐ An oath or declaration of the inventor(s) (35 U.S.C. 371(c)(4)).
10. ☐ A translation of the annexes to the International Preliminary Examination Report under PCT Article 36 (35 U.S.C. 371(c)(5)).

Items 11. to 16. below concern document(s) or information included:

11. ☒ An Information Disclosure Statement under 37 CFR 1.97 and 1.98.
12. ☐ An assignment document for recording. A separate cover sheet in compliance with 37 CFR 3.28 and 3.31 is included.
13. ☒ A FIRST preliminary amendment.
☐ A SECOND or SUBSEQUENT preliminary amendment.
14. ☐ A substitute specification.
15. ☐ A change of power of attorney and/or address letter.
16. ☒ Other items or information:
 - 1) Certificate of Mailing under 37 C.F.R. 1.10;
 - 2) Transmittal of Information Disclosure Statement under 37 C.F.R. 1.97(b);
 - 3) Information Disclosure Citation (Modified Form PTO-1449) and references cited therein; and
 - 4) Return Receipt Post Card.

Date of Deposit: MAR 16 2001

Express Mail Label No. EK662544851US

U.S. APPLICATION NO. (If known, see 37 CFR 1.5)

097787229

INTERNATIONAL APPLICATION NO
PCT/EP99/06882ATTORNEY'S DOCKET NUMBER
LEA 33 25317. ☒ The following fees are submitted:**BASIC NATIONAL FEE (37 CFR 1.492 (a) (1) - (5)):**

Neither international preliminary examination fee (37 CFR 1.482)
nor international search fee (37 CFR 1.445(a)(2)) paid to USPTO
and International Search Report not prepared by the EPO or JPO \$970.00

International preliminary examination fee (37 CFR 1.482) not paid to
USPTO but International Search Report prepared by the EPO or JPO \$840.00

International preliminary examination fee (37 CFR 1.482) not paid to USPTO but
international search fee (37 CFR 1.445(a)(2)) paid to USPTO \$690.00

International preliminary examination fee paid to USPTO (37 CFR 1.482)
but all claims did not satisfy provisions of PCT Article 33(1)-(4) \$670.00

International preliminary examination fee paid to USPTO (37 CFR 1.482)
and all claims satisfied provisions of PCT Article 33(1)-(4) \$96.00

ENTER APPROPRIATE BASIC FEE AMOUNT =

CALCULATIONS PTO USE ONLY

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Surcharge of \$130.00 for furnishing the oath or declaration later than ☐ 20 ☐ 30
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\$

CLAIMS	NUMBER FILED	NUMBER EXTRA	RATE
Total claims	9 - 20 =	0	X \$18.00
Independent claims	1 - 3 =	0	X \$78.00
MULTIPLE DEPENDENT CLAIM(S) (if applicable)		0	+ \$260.00

\$ 0.00

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TOTAL OF ABOVE CALCULATIONS =

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Reduction of 1/2 for filing by small entity, if applicable. A Small Entity Statement
must also be filed (Note 37 CFR 1.9, 1.27, 1.28).

\$

SUBTOTAL =

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Processing fee of \$130.00 for furnishing the English translation later than ☐ 20 ☐ 30
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\$

TOTAL NATIONAL FEE =

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Fee for recording the enclosed assignment (37 CFR 1.21(h)). The assignment must be
accompanied by an appropriate cover sheet (37 CFR 3.28, 3.31). \$40.00 per property +

\$

TOTAL FEES ENCLOSED =

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Amount to be
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a. ☐ A check in the amount of \$ _____ to cover the above fees is enclosed.

b. ☒ Please charge my Deposit Account No. 13-3372 in the amount of \$ 860.00 to cover the above fees.
A duplicate copy of this sheet is enclosed.

c. ☒ The Commissioner is hereby authorized to charge any additional fees which may be required, or credit any
overpayment to Deposit Account No. 13-3372. A duplicate copy of this sheet is enclosed.

NOTE: Where an appropriate time limit under 37 CFR 1.494 or 1.495 has not been met, a petition to revive (37 CFR 1.137(a) or (b)) must be filed and granted to restore the application to pending status.

SEND ALL CORRESPONDENCE TO

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NAME

41,670

REGISTRATION NUMBER

PATENT
Atty. Docket No.: Le A 33 253

IN THE UNITED STATES PATENT AND TRADEMARK OFFICE

APPLICANTS: Kanikanti, *et al.*

SERIAL NO.: National Stage Application of PCT/EP99/06882

FILING DATE: herewith

TITLE: Multiple Unit Controlled Food Effect-Independent Release
Pharmaceutical Preparations and Method for Preparing the Same

PRELIMINARY AMENDMENT

Box PCT
Assistant Commissioner for Patents
Washington, D.C. 20231

Sir:

This Preliminary Amendment is submitted in the national stage application for PCT/EP99/06882. Please amend the application as follows:

In the Claims

Please cancel claims 9-11.

Remarks

By way of this Amendment, claims 1-8 and 12 are pending. Claims 9-11 have been canceled.

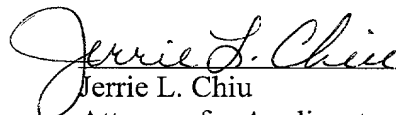
Conclusion

Applicants respectfully submit that the pending claims are in condition for allowance. Please charge any fees due with this amendment to deposit account number 13-3372. If the Examiner believes that a conversation with Applicants' attorney would be helpful in expediting prosecution of this application, the Examiner is invited to call the undersigned attorney at (203) 812-3964.

Respectfully submitted,

Dated: March 9, 2001

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Agitation-independent pharmaceutical multiple-unit sustained-release preparations and processes for their production

5 The present invention relates to orally administrable multiple-unit sustained-release dose forms having controlled and agitation-independent release and processes for their production using a selected erodable hydrophilic polymer.

10 For many medicaments, it is desirable that they guarantee a controlled, long-lasting and uniform release of the active compound after administration once daily. In this way, the desired plasma concentration can be maintained over a relatively long period without great variations and thus the medicament safety and the patient compliance are increased. Formulations which release the active compound over a defined period in this manner are called sustained-release formulations. Various techniques
15 for their production are already known.

Very often, single-unit matrix tablets which contain the active compound in a matrix of polymers and some pharmaceutical excipients are employed for this purpose. The polymer can either be hydrophilic or hydrophobic or a mixture thereof. Meanwhile,
20 matrix tablets containing hydrophilic polymers have become very popular, since these are comparatively inexpensive, non-toxic, processable in conventional plants, etc.

A further method is the coating of preparation forms with buffered or pH-dependent
25 coatings which are intended to guarantee a controlled release in certain areas of the gastrointestinal tract.

While the erosion matrix tablets are susceptible to mechanical stress, in particular hydrodynamic stresses, the pH-controlled formulations are susceptible to pH changes
30 in the gastrointestinal tract. While the tablet moves through the gastrointestinal tract, both the pH and the mechanical stress vary, in particular also as a function of the

nature and amount of the filling of the stomach and of the digestive tract. This dependence of the active compound release is called the "agitation dependence" or the "food effect". It is seen that the release rate of most sustained-release formulations is dependent on the food intake and thus different profiles of action occur depending on whether the medicament is taken before, during or after a meal.

There have been numerous attempts to exclude or to minimize the undesirable variability of this "food effect". For erosion-controlled preparations, an approximately agitation-independent single-unit system has been described which, however, is technically very complicated and therefore impracticable (cf. W.D. Lindner et al. Farm., 51 (1996) 263). As a further possibility of an agitation-independent preparation, a single-unit osmotic pump system has been described and in some cases successfully marketed. Here, the active compound is squeezed outwards through defined openings or pores of a chamber, the squeezing pressure being produced by a swelling polymer whose water absorption is osmotically controlled (cf. US Patent 4 449 983, US Patent 4 203 400 and US Patent 4 327 725).

The problems and disadvantages of the previously proposed and employed agitation-independent sustained-release formulations are known and presented, inter alia, in the description of EP 0 425 298.A2. According to this application, it is attempted to achieve the agitation independence of salt-forming active compounds by means of different coatings with poorly soluble polymers. The disadvantages of this process likewise lie in the technically complicated process measures and in the fact that only certain salt-forming and thus easily soluble active compounds can be employed.

Multiple-unit formulations are designated as those formulations which, in contrast to so-called single-unit formulations such as tablets, consist of a number of small particles, e.g. pellets, granules, minitables or grains which are contained, for example, in a capsule. In the gastrointestinal tract, these particles are then present independently of one another. Such multiple-unit formulations have a number of advantages in comparison to single-unit formulations. They provide for a more uniform absorption

of the active compound and for smaller inter- and intraindividual variations of the pharmacokinetic profiles. Furthermore, different active compounds and dosages can thus be simply inserted, for example, into capsules. These formulations can thus be tailored to the different medicinal requirements without a great outlay.

5

The object of the present invention is to be seen as making available agitation-independent multiple unit sustained-release formulations, i.e. formulations without an interfering food effect, which can be produced in a simple manner for all types of active compounds, in particular for poorly soluble active compounds.

10

Multiple-unit sustained-release formulations according to the present invention are formulations which, in the USP paddle test using apparatus II, release 80% of the active compound within 4 to 14 hours, preferably within 6 to 12 hours, relative to the total amount of active compound in the formulation.

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Agitation-independent formulations according to the present invention are those which, in the USP XXII paddle test with 900 ml of release medium, pH 6.8 at a stirren speed of 50 rpm and of 150 rpm, have a maximum release difference of $\pm 10\%$, preferably $\pm 5\%$.

20

The stirren speed of the paddle test according to USP was selected with regard to the publication B. Abrahamsson et al., Eur. J. Pharm. Sci., 46 (1998) 69, according to which the mechanical stress of a tablet in the gastrointestinal tract is to be compared, for example, with the conditions which correspond to a stirring motion in the paddle

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This object can be achieved according to the invention in that

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- a) the hydrophilic polymer employed is hydroxypropylcellulose (HPC) having an average molecular weight of 250 000 to 1 200 000, preferably 350 000 to 1 150 000, in an amount from 40 to 95% by weight, preferably 45 to 90% by

weight, based on the active compound-polymer mixture, and a molar degree of substitution of ≥ 3 as a release-sustaining erosion material and

- 5 b) the active compound-polymer combination is converted into small particles such as pellets, granules or minitables having a maximum diameter of 0.2 to 3.0 mm, preferably of 0.5 to 2 mm.

HPC having an average molecular weight of 700 000 to 1 200 000, preferably 850 000 to 1 150 000, can also be employed.

10

Maximum diameter is here understood as meaning the greatest longitudinal dimension of the particle; according to the invention it is 0.2 to 3 mm.

15

If desired, the miniparticles can be lacquered and further customary pharmaceutical excipients can also be added.

20

These sustained-release miniparticles can be produced and administered in a simple manner in the desired dose units as multiple-unit sustained-release dose forms, e.g. in hard gelatin capsules, as sachets or are modified to give tablets which decompose into the miniparticles again immediately after administration and thus behave like a multiple-unit dose form.

25

With knowledge of the prior art, it was not obvious that, as a result of the selection of the abovementioned erodable hydrophilic polymer HPC and simultaneous limitation of the maximum size of the active compound-containing polymer particles to at most 3 mm diameter, an agitation-independent sustained-release formulation can be produced. It was rather to be expected that erodable hydrophilic polymers especially would exhibit a particularly strong agitation effect or food effect. It is known, for example, that nifedipine-containing matrix tablets having diameters of 9 or 10 mm, which contain HPC or HPMC (hydroxypropylmethylcellulose) as hydrophilic poly-

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mer, are strongly agitation-dependent and exhibit a strong food effect (cf. Adalat CC®; EP 0 299 211 and B. Abrahamsson et al., J. Controlled Rel., 52 (1998) 301).

5 On the other hand, minitabets for oral administration have been known and described for some time (cf. Colombo et al., Acta Technol. Legis. med. 1992, 3 (3), 137). However, it was previously not known that the particles according to the invention having a maximum diameter of 3 mm are agitation-independent sustained-release formulations.

10 To achieve the object according to the invention, the combination of both elements a) and b) is necessary. Some experiments with minierosion tablets which contain nifedipine as active compound and which do have a diameter of 2 mm, but contain a mixture of hydroxyethylcellulose (HEC) and hydroxypropylmethylcellulose (HPMC) as erodable polymer, show a significant agitation dependence.

15 Surprisingly, it has been found that, as a result of the combination of the selection of the erodable hydrophilic polymer HPC and the reduction of the size of the miniparticles to be employed to at most 3 mm diameter, agitation-independent multiple-unit sustained-release formulations can be obtained in a simple and effective manner.

20 According to informative tests, the formulations according to the invention showed virtually no food dependence.

25 The pellets, granules, minitabets or grains used according to the invention are produced according to customary methods. In addition to the conventional formulation methods, in which HPC is granulated with the active compound and, if appropriate, further excipients using water or organic solvents, the use of melt extrusion methods can also be employed advantageously. Such melt extrusion methods have been known for a long time. Variations of this melt extrusion are also proposed in the
30 more recent patent literature (cf. DE 195 04 831.8, EP 240 904, US-PS 5 456 923, EP 544 144 and in particular WO 96/25149).

Many of the previously known methods of melt extrusion have a number of disadvantages compared with the methods employable according to the invention. Thus, for the production of an extrudate, at least two polymers, e.g. a water-soluble polymer and a water-insoluble polymer, are often used. Owing to the necessity of additional plasticizers or other excipients, the ratio excipient/pharmaceutical can be unfavourably influenced, so that the finished product is very voluminous and also expensive. According to the present invention, the agitation- and food-independent formulations can be obtained even by simple mixing and extrusion of the desired active compound with HPC.

If desired, further excipients can of course also be employed for the multiple-unit sustained-release formulations according to the invention, e.g. magnesium stearate or film coatings or lacquers which prevent the sticking together of the particles. These excipients, however, have no direct influence on the sustained-release action of the preparation according to the invention, which is agitation-independent or has no food effect.

It is also possible to employ for the preparation of the minitabets in addition to the essential polymer HPC further hydrophilic and water-insoluble polymers, e.g. polymethacrylate esters. An example is the known ammonio methacrylate copolymer type B (Eudragit® RS PO).

The present invention also relates to processes for the production of multiple-unit sustained-release dose forms, characterized in that at least one therapeutically active substance and HPC having an average MW of 250 000 to 1 200 000 as a hydrophilic thermoplastic, but pharmaceutically acceptable polymer and also, if appropriate, further customary pharmaceutical excipients which, however, do not contribute to the sustained-release effect, are mixed, granulated and tableted or mixed, extruded and granulated to give particles having a maximum particle diameter of 3 mm and these are then converted into a suitable oral administration form.

In the extrusion process, therapeutically active pharmaceuticals and the polymer are conveyed either simultaneously, without prior mixing, or as a mixture, after prior mixing, into a normal extruder, preferentially a double-screw extruder, which has
5 been heated beforehand to a temperature at which the polymer and the pharmaceutical are not degraded. The temperature range at the outlet nozzle of the extruder here is 50 to 220°C, preferably 80 to 210°C and particularly 100-180°C. In the area of the product inlet into the extruder, the temperature is around 25°C. The temperature in the intermediate area of the extruder is between the temperature in the product inlet
10 area of the extruder and the temperature at the outlet nozzle of the extruder.

The homogeneous mixture softens during passage through the extruder and is pressed at the end through a plate which contains at least one nozzle having a defined diameter of about 0.2 to 3.0 mm, preferably of 0.5 to 2.0 mm. The extruded strands,
15 which on emergence from the extruder nozzle are still soft and rapidly become solid at room temperature, are cut to give granules having a particle diameter of about 0.2 to 3 mm, preferably 0.5 to 2 mm, directly after their emergence. Alternatively, the extruded strands are immediately (on-line) granulated (e.g. water-ring granulation or underwater granulation or air granulation) or immediately cut into pieces. Air granu-
20 lation is preferred. The extrudates obtained can be filled directly into hard gelatin capsules. As a particular embodiment, it has proved advantageous additionally to lacquer the extrudates obtained before filling them into gelatin capsules, preferably using a water-insoluble but water-permeable and non-gel-forming polymer.

25 This sustained-release dose form according to the present invention is not susceptible to mechanical stress or hydrodynamic stress in the gastrointestinal tract; the rate of the active compound release therefore does not depend on the mechanical stress and the hydrodynamic stress to which the product is exposed and is independent of the degree of filling of the stomach. The sustained-release dose form thus exhibits no
30 food effect.

The lacquered extrudates can be compressed with conventional excipients (e.g. microcrystalline cellulose, Ac-Di-Sol[®] etc.) to give tablets. These tablets decompose rapidly after their administration, so that the tablet behaves as a multi-unit dose form.

5

The formulation according to the present invention can also be produced using known tableting processes, in which the ingredients are granulated, for example, in a known manner, made glidable and compressed to give microtablets of a diameter of ≤ 3 mm, preferably of ≤ 2 mm.

10

In contrast to the formulations according to the prior art, the agitation-independent sustained release is achieved, as already mentioned, in the present invention by the combination a) of the polymer HPC used and b) the maximum diameter, whilst the coating only serves to protect the dose form from sticking.

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The active compounds used can be any desired orally administrable pharmaceuticals, e.g. anti-infectives, circulatory agents, antimycotics, antidepressants, antimentia agents, antiepileptics, anti-inflammatories, analgesics, antiasthmatics, antithrombotics, antitumour agents, antimalaria agents, non-steroidal antiinflammatory agents (NSAID), diuretics, antiarrhythmics, blood sugar-lowering agents, ACE inhibitors, sedatives, decongestants, antihistamines or hypolipidaemics. Hypolipidaemics can be, inter alia, Apo B inhibitors or MTP inhibitors. Of particular interest are the Apo B inhibitors according to EP 705 831, to which reference is expressly made here. Of very particular interest is the substance 2-cyclopentyl-2-[4-(2,4-dimethyl-pyrido[2,3-b]indol-9-yl-methyl)-phenyl]-N-(2-hydroxy-1-phenyl-ethyl)acetamide. For the purposes of the present invention, only those pharmaceuticals are incorporated which do not decompose under the temperatures and processing conditions. The amount of active compound to be administered per dose unit can be varied depending on the nature of the pharmaceutical and the release rate. It has proved advantageous to employ 0.8 to 10 parts by weight, preferably 1 to 5 parts by weight, of the gel-forming polymer to one part by weight of active compound.

25

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In contrast to the previously known techniques, only a single polymer is needed for sustained release according to the present invention. The desired release rate is obtained by variation of the production parameters. The pharmaceutical release rate is, for example, influenced by the pharmaceutical concentration in the final product or by process parameters of the extrusion, such as the screw geometry, the extrusion rate, the extrusion temperature, the diameter and the surface area of the extrudate, the viscosity and molecular weight of the polymer, etc.

As already mentioned, further customary excipients can also be used which are customary in the production of solid dose forms in pharmacy and are known from the literature. None of these excipients is necessary, however, in order significantly to influence the desired retardation of the release of the pharmaceutical and the agitation independence according to the invention. These excipients rather only serve to make the process more flexible.

The extrudates or minitables are optionally lacquered, for example, with pH-independent aqueous dispersions such as an ethylcellulose dispersion (e.g. Aquacoat EC 30 trade mark of FMC) or of a poly(ethyl acrylate, methyl methacrylate) 2:1 (e.g. Eudragit NE 30 D trade mark of Röhm Pharma). Moreover, a plasticizer such as triethyl citrate or Tween 20 can be used in order that the lacquer film does not become brittle during storage. Magnesium stearate can additionally be incorporated into the lacquer suspension as an antiadhesive agent. HPMC serves as the pore former. The lacquer essentially has no influence on the release rate, except that a retardation of the commencement of release (lag time) can occur during the first 1-2 hours after the administration.

Typical lacquer suspensions for minitables and extrudates which may be mentioned are: (all data in % by weight)

A. 30-60% (preferably 40%) of Eudragit® NE 30 D dispersion; 3-10% (preferably 5%) of HPMC 3 cP; 0.05-0.5% (preferably 0.1%) of Tween 20; 1-7.5% (preferably 2.5%) of magnesium stearate and completely deionized water to 100%.

5

B. 15-30% (preferably 25%) of Aquacoat® EC 30 D dispersion; 3-10% (preferably 4-5%) of HPMC 15 cP; 0.5-4% (preferably 2%) of triethyl citrate and completely deionized water to 100%.

10 The lacquer suspensions, for example, are prepared by first dissolving HPMC and the plasticizer separately in water and then mixing them with the dispersion of the film former. In the presence of magnesium stearate, this is dispersed in the aqueous solution of HPMC and plasticizer before the addition of the Eudragit NE 30 D dispersion.

15 The optionally lacquered particles of the active compound-polymer combination according to the invention, such as pellets, granules, minitabets or grains, can be filled into capsules, pressed to give tablets or further processed to give other known administration forms or finished medicaments according to customary methods.

20 The invention is illustrated in greater detail by means of the following examples.

Influence of paddle agitation on the active compound release

5 The active compound release from Examples 16 and 17 according to the invention and from the Comparison Example A over time was investigated in a USP XXII paddle test. It was seen here that in Examples 16 and 17 the active compound release at 50 and 150 revolutions per minute (rpm) lay apart by at most 5% over a period of 14 hours (i.e. up to complete release), whilst in Comparison Example A release differences of up to 50% occurred.

10 **Comparison Example A**

19.4 parts by weight of hydroxypropylmethylcellulose (viscosity 100 000 cP, type 2208) and 45.3 parts by weight of hydroxyethylcellulose (viscosity 15 000 cP) are granulated with an aqueous suspension of nifedipine (30 parts by weight) and hydroxypropylcellulose (2 parts by weight) of a viscosity of <10 cP. The granules obtained are made glidable with magnesium stearate and compressed to give 2 mm minitabets of 6.4 mg. The minitabets are lacquered in a conventional manner with an aqueous dispersion of Eudragit NE 30 D, magnesium stearate, Tween 20®, hydroxypropylmethylcellulose 3 cP and water. Per kg of minitabets, 0.6 kg of lacquer suspension A is sprayed on. Some lacquered minitabets containing an equivalent of 30 mg of nifedipine are encapsulated.

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Working Examples

Example 1

5 3 kg of the pharmaceutical nifedipine are mixed with 7 kg of highly viscous HPC
(MW 400 000 from Nippon Soda, Japan). The mixture is processed in a double-
screw extruder with two outlet nozzles having a diameter of 2 mm. The material is
extruded at a nozzle temperature of 150°C. The temperature of the various subunits
10 in the extruder cylinder is adjusted to a temperature which lies at least approximately
10°C below the nozzle temperature. The extrudate is cut into cylinders approximately
2 mm long and lacquered in a fluidized bed lacquering unit. Per kg of extrudate,
0.6 kg of the lacquer suspension A is sprayed on. The lacquering is carried out under
customary conditions.

15 **Example 2**

Analogous to Example 1, but 2 kg of nifedipine are mixed with 8 kg of the same
polymer type.

20 **Example 3**

Analogous to Example 1, but the nozzle temperature is 160°C.

Example 4

25

Analogous to Example 1, but the nozzle diameter is 1.4 mm.

Example 5

30

Analogous to Example 1, but the nozzle diameter is 0.8 mm.

Example 6

Analogous to Example 1, but the extruded strands were first cut into cylinders approximately 3 mm long.

5

Example 7

Analogous to Example 1, but the cylinders cut approximately 2 mm long were not lacquered.

10

Example 8

Analogous to Example 1, but the nozzle temperature is 140°C.

15

Example 9

Analogous to Example 1, but the polymer used is HPC having an average molecular weight of about 850 000 (Hercules, USA).

20

Example 10

Analogous to Example 1, but the polymer used is HPC having an average molecular weight of about 1 000 000 (Hercules, USA).

25

Example 11

Analogous to Example 1, but the pharmaceutical used is nisoldipine.

Example 12

5 Analogous to Example 1, but the pharmaceutical used is nimodipine, HPC (MW 400 000, Nippon Soda, Japan) is employed, and the nozzle temperature is 110°C.

Example 13

10 The same composition as in Example 1 is extruded under the same extrusion conditions in a commercially obtainable extrusion and granulation apparatus and then immediately granulated by means of the water ring process and dried. The resulting extrudate was slightly rounded and, as a result, more easily processable.

Example 14

15 The same composition as in Example 1 is extruded in a commercially obtainable extrusion apparatus having a nozzle plate of 40×0.8 mm or 36×1.3 mm drillings, and then immediately on-line granulated and dried by air granulation. The resulting extrudates were more easily processable. The granules were lacquered as in Example 1.
20

Example 15

25 The same composition as in Example 1 is extruded through an extruder with outlet nozzles having a diameter of 1 mm, and the extruded strand is cooled by spraying with water and immediately granulated and dried. The extrudates obtained are further processed as described in Example 1.

Example 16

250 parts (by weight) of hydroxypropylcellulose (MW 1 000 000; viscosity 1 500 to
3 000 cP (1% w/v; 25°C)) are granulated with an aqueous suspension of nifedipine
5 (30 parts) and hydroxypropylcellulose (2 parts). The resulting granules are made
glidable with magnesium stearate (1.5 parts) and compressed to give 2 mm
minitablets of 6.5 mg. The minitablets are lacquered in a conventional manner with
an aqueous dispersion of Eudragit NE 30 D, magnesium stearate, Tween 20®, hy-
droxypropylmethylcellulose 3 cP and water. Per kg of minitablets, 0.6 kg of lacquer
10 suspension A is sprayed on. Some lacquered minitablets are encapsulated with an
equivalent of 30 mg of nifedipine.

Example 17

15 Hydroxypropylcellulose corresponding to Example 16 (42.6 parts) is mixed with
Eudragit® RS PO (40.8 parts) and granulated with an aqueous suspension of nifed-
ipine (30 parts) and hydroxypropylcellulose (2 parts) of a viscosity of <10 cP. The
resulting granules are made capable of gliding with magnesium stearate (1.5 parts)
and compressed to give 2 mm minitablets of 6.5 mg. The minitablets (2 mm diame-
20 ter) are lacquered analogously to Example 16.

Example 18

1 kg of 2-cyclopentyl-2-[4-(2,4-dimethyl-pyrido[2,3-b]indol-9-yl-methyl)-phenyl]-N-
25 (2-hydroxy-1-phenyl-ethyl)acetamide are mixed with 2 kg of HPC (MW 250 000-
400 000, Nippon Soda, Japan). The mixture is processed in a double-screw extruder
with two outlet nozzles having a diameter of 2 mm. The material is extruded at a
nozzle temperature of 215°C. The extrudate is cut into cylinders approximately 2 mm
long and lacquered in a fluidized bed lacquering unit analogously to Example 1.
30

If not expressly stated otherwise, the term “parts” in the present application should always be understood as meaning “parts by weight”.

Patent Claims

1. Process for the production of an orally administrable multiple-unit sustained-release dose formulation having controlled agitation-independent release,
5 characterized in that the hydrophilic polymer HPC having an average molecular weight of 250 000 to 1 200 000 is combined in an amount from 40 to 95% by weight, based on the active compound-polymer mixture and a molar degree of substitution of at least 3, as a release-sustaining erosion material, with at least one pharmaceutical active compound and this active compound-
10 polymer combination is converted into small particles having a diameter of 0.2 to 3.0 mm and these are used in the production of active oral administration forms and finished medicaments.
2. Process for the production of a formulation according to Claim 1, characterized
15 in that HPC is employed in an amount from 45 to 90% by weight.
3. Process for the production of a formulation according to Claim 1, characterized
in that HPC having an average molecular weight of 350 000 to 1 150 000 is employed.
20
4. Process for the production of a formulation according to Claim 1, characterized
in that the active compound-polymer combination is converted into small particles having a maximum diameter of 0.5 to 2 mm.
- 25 5. Process for the production of formulations according to Claim 1, characterized
in that the particles for the active compound-polymer combination are produced by melt extrusion and granulation.
6. Process for the production of formulations according to Claim 1, characterized
30 in that the particles of the active compound-polymer combination are produced by conventional tableting methods.

- 5 7. Process for the production of formulations according to Claim 1, characterized in that the active compound-polymer combination particles are produced in the form of pellets, granules, minitabets or grains and these are filled into capsules in an efficacious dosage.
- 10 8. Process for the production of formulations according to Claim 1, characterized in that the active compound-polymer combination particles are additionally lacquered.
9. Use of HPC having an average molecular weight of 250 000 to 1 200 000 in the production of agitation-independent pharmaceutical sustained-release preparations, obtainable according to Claim 1.
- 15 10. Use of HPC having an average molecular weight of 350 000 to 1 150 000 as main sustained-release polymer and, if appropriate, small amounts of further hydrophilic polymers such as polymethacrylic esters in the production of agitation-independent sustained-release preparations according to Claim 1.
- 20 11. Use of active compound-polymer combination particles according to Claim 1 for the production of finished medicaments in the form of capsules or tablets.
12. Orally administrable multiple-unit sustained-release dose formulations having controlled agitation-independent release obtainable according to Claim 1.

Agitation-independent pharmaceutical multiple-unit sustained-release preparations and processes for their production

A b s t r a c t

The present invention relates to orally administrable multiple-unit sustained-release dose forms having controlled agitation-independent release of active compound and processes for their production using a selected erodable hydrophilic polymer (HPC) and a limitation of the maximum size of the active compound-containing polymer particles to ≤ 3 mm.

COMBINED DECLARATION AND POWER OF ATTORNEY

ATTORNEY DOCKET NO

Le A 33 253

As a below named inventor, I hereby declare that:

My residence, post office address and citizenship are as stated below next to my name. I believe I am the original, first and sole inventor (if only one name is listed below) or an original, first and joint inventor (if plural names are listed below) of the subject matter which is claimed and for which a patent is sought

on the invention entitled

"MULTIPLE UNIT CONTROLLED FOOD EFFECT-INDEPENDENT RELEASE PHARMACEUTICAL PREPARATIONS AND METHOD FOR PREPARING THE SAME"

the specification of which is attached hereto,

or was filed on **September 17, 1999**

as a PCT Application Serial No. **PCT/EP99/06882**

I hereby state that I have reviewed and understand the contents of the above-identified specification, including the claims.

I acknowledge the duty to disclose information which is material to the patentability of this application in accordance with Title 37, Code of Federal Regulations, §1.56.

I hereby claim foreign priority benefits under Title 35, United States Code, §119 of any foreign application(s) for patent or inventor's certificate listed below and have also identified below any foreign application for patent or inventor's certificate having a filing date before that of the application on which priority is claimed:

Prior Foreign Application(s), the priority(ies) of which is/are to be claimed:

198 42 753.0
(Number)

Germany
(Country)

September 18, 1998
(Month/Day/Year Filed)

I hereby claim the benefit under Title 35, United States Code, §120 of any United States application(s) listed below and, insofar as the subject matter of each of the claims of this application is not disclosed in the prior United States application in the manner provided by the first paragraph of Title 35, United States Code, §112, I acknowledge the duty to disclose the material information as defined in Title 37, Code of Federal Regulations, §1.56 which occurred between the filing date of the prior application and the national or PCT international filing date of this application:

(Application Serial No.)	(Filing Date)	(Status)
		(patented, pending, abandoned)

(Application Serial No.)	(Filing Date)	(Status)
		(patented, pending, abandoned)

I hereby declare that all statements made herein of my own knowledge are true and that all statements made on information and belief are believed to be true; and further that these statements were made with the knowledge that willful false statements and the like so made are punishable by fine or imprisonment, or both, under Section 1001 of Title 18 of the United States Code and that such willful false statements may jeopardize the validity of the application or any patent issued thereon.

Le A 33 253-US

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